

PCT

WORLD INTELLECTUAL PROPERTY ORGANIZATION
International Bureau



INTERNATIONAL APPLICATION PUBLISHED UNDER THE PATENT COOPERATION TREATY (PCT)

(51) International Patent Classification 7 : A61K 6/083		A1	(11) International Publication Number: WO 00/61073 (43) International Publication Date: 19 October 2000 (19.10.00)
(21) International Application Number: PCT/US00/08709 (22) International Filing Date: 31 March 2000 (31.03.00)		(81) Designated States: JP, European patent (AT, BE, CH, CY, DE, DK, ES, FI, FR, GB, GR, IE, IT, LU, MC, NL, PT, SE). Published <i>With international search report.</i>	
(30) Priority Data: 60/128,734 12 April 1999 (12.04.99) US Not furnished 31 March 2000 (31.03.00) US			
(71) Applicant: DENTSPLY INTERNATIONAL INC. [US/US]; 570 West College Avenue, P.O. Box 872, York, PA 17404-0872 (US).			
(72) Inventors: BLACKWELL, Gordon, B.; Hegaublick 28, D-78365 Konstanz (DE). UTZ, Karin; Stifterstrasse 51, D-78467 Konstanz (DE).			
(74) Agents: HURA, Douglas, J. et al.; Dentsply International Inc., 570 West College Avenue, P.O. Box 872, York, PA 17404-0872 (US).			
(54) Title: DENTAL COMPOSITE RESTORATIVE MATERIAL AND METHOD OF RESTORING A TOOTH			
(57) Abstract			
<p>A composite material is provided which, while having an unusually high filler content may be extruded from a dental syringe and remains easily adaptable in the dental cavity. When materials of the present invention are cured, dental restorations are provided which have unusually high surface hardness and yield strength, as well as a low volume shrinkage on curing. This is achieved by use of a mixture of filler particles with a specific size, size range, and size relationship. Such a combination of properties makes the material of the present invention particularly useful for restoring cavities in posterior teeth.</p>			

FOR THE PURPOSES OF INFORMATION ONLY

Codes used to identify States party to the PCT on the front pages of pamphlets publishing international applications under the PCT.

AL	Albania	ES	Spain	LS	Lesotho	SI	Slovenia
AM	Armenia	FI	Finland	LT	Lithuania	SK	Slovakia
AT	Austria	FR	France	LU	Luxembourg	SN	Senegal
AU	Australia	GA	Gabon	LV	Latvia	SZ	Swaziland
AZ	Azerbaijan	GB	United Kingdom	MC	Monaco	TD	Chad
BA	Bosnia and Herzegovina	GE	Georgia	MD	Republic of Moldova	TG	Togo
BB	Barbados	GH	Ghana	MG	Madagascar	TJ	Tajikistan
BE	Belgium	GN	Guinea	MK	The former Yugoslav Republic of Macedonia	TM	Turkmenistan
BF	Burkina Faso	GR	Greece	ML	Mali	TR	Turkey
BG	Bulgaria	HU	Hungary	MN	Mongolia	TT	Trinidad and Tobago
BJ	Benin	IE	Ireland	MR	Mauritania	UA	Ukraine
BR	Brazil	IL	Israel	MW	Malawi	UG	Uganda
BY	Belarus	IS	Iceland	MX	Mexico	US	United States of America
CA	Canada	IT	Italy	NE	Niger	UZ	Uzbekistan
CF	Central African Republic	JP	Japan	NL	Netherlands	VN	Viet Nam
CG	Congo	KE	Kenya	NO	Norway	YU	Yugoslavia
CH	Switzerland	KG	Kyrgyzstan	NZ	New Zealand	ZW	Zimbabwe
CI	Côte d'Ivoire	KP	Democratic People's Republic of Korea	PL	Poland		
CM	Cameroon	KR	Republic of Korea	PT	Portugal		
CN	China	KZ	Kazakhstan	RO	Romania		
CU	Cuba	LC	Saint Lucia	RU	Russian Federation		
CZ	Czech Republic	LI	Liechtenstein	SD	Sudan		
DE	Germany	LK	Sri Lanka	SE	Sweden		
DK	Denmark	LR	Liberia	SG	Singapore		
EE	Estonia						

DENTAL COMPOSITE RESTORATIVE MATERIAL AND METHOD OF RESTORING A TOOTH

Background to the invention

Dental composites, which essentially comprise a mixture of a polymerizable resin and a glassy filler, have been developing since the early 1970's, when the first materials of this class were introduced. See for example R.L. Bowen et al., "A new series of X-ray-opaque reinforcing fillers for composite materials, J. Dental Research, vol. 51(1) 1972. Until this time, fillings had been based on silver-mercury amalgams, mixtures of acid leachable glass with phosphoric acid (known as "silicate cements"), or unfilled polymerizable resins, and each class of material has certain strengths and weaknesses. For instance, amalgams are generally considered to be cheap and easy to use, and to have a long lifetime due to their strength and high resistance to wear. Disadvantages of amalgam are toxicity of the mercury and the black colour of the filling. Silicate fillings were approximately tooth coloured and released fluoride into the tooth to help prevent a recurrence of decay. However they tended to dissolve quickly and were weak, and are barely used nowadays. Unfilled resins brought advantages of toughness, convenience, and aesthetics, but were still weak, limiting their use to areas of low stress. These unfilled resins also have a high volume shrinkage, commonly at least 5%. This leads to formation of gaps between the filling and the tooth, and subsequent recurring decay of the tooth around and underneath the restoration. The introduction of composite materials brought improvements in surface hardness, higher physical strengths, good aesthetics, lower shrinkage, and also higher resistance to wear. However the

wear rate of these composite materials is still higher than that of amalgam, and their shrinkage of around 2 to 3 volume percent still leads to gap formation and recurrent caries. It is an aim of many researchers in the dental area to develop composite materials with higher strength, reduced shrinkage and higher resistance to wear, which may be used in place of amalgam. Preferably the material should also be extrudable from a dental syringe since this procedure is not only convenient and time saving for the dentist, but also helps to avoid the inclusion of air bubbles in the cavity.

The present invention provides composite materials with low shrinkage and high surface hardness, and a method for preparing these composite materials. Within certain ranges of the invention materials are provided which may also be extruded from a dental syringe designed for this use.

Prior Art

Composite materials for dental use and general methods for making them have been known for many years. See for example BP1401805, US3740850, US4215033, and US3801344. These patents essentially describe mixtures of acrylate resins with glass or various metal oxides as filler and claim, for example, the advantages of natural colour and desirable hardness. Although an improvement at the time, these early materials were still relatively weak and had low resistance to wear. Improvements in surface hardness were achieved when milling procedures improved and fillers with smaller particle sizes became available. Attempts were also made to use different types of monomer, for instance a silane containing monomer as in US4504231, or a mixture of monomers as in US5730601. However the shrinkage of these materials still remained too high, at around 2 to 3 percent

by volume. Further improvements were made by the inclusion of two or more types of filler particle, for example a conventional glass fillers with particle size ranges of 0.5 to 40 microns and 0.2 to 15 microns, together with a fine filler with particle size in the range 5 to 150 nano metres, as in US4649165. These materials however still have the problem that it is hard to incorporate sufficient filler into the composite to obtain the desired hardness. Attempts to overcome this problem have also included the use of surfactants, as in USP 4,374,937. However there remains the problem that use of too much conventional filler material in a composite leads to a stiff paste which is hard to manipulate, and ultimately to a dry and non-cohesive mixture. It is desirable to be able to extrude a dental filling material directly from a syringe into the tooth cavity, and this is not possible with such stiff pastes. Such pastes when cured typically have a yield strength around 130 MPa, a surface Vickers hardness of about 70, and a volume shrinkage between 2.5 to 3 percent. The yield strength is the maximum load that may be applied to a material before permanent deformation and damage occurs, and it is desirable that this is as high as possible. A high surface hardness is needed because this reduces abrasive wear of the material, while low shrinkage is desirable in order to minimise gap formation around a filling.

Detailed Description of the invention

In the present invention it has been found that by the use of filler combinations with a certain defined size distribution and size relationship, an unexpectedly high amount of filler may be combined with the resin matrix without the paste becoming either stiff and hard to handle, or crumbly and non-cohesive. The resulting pastes when cured have a yield strength of at least 180 MPa, a Vickers hardness of over 90, and a volume shrinkage on

curing less than 2%. A conventionally made composite paste commonly contains ground glass particles with a particle distribution of about 0.05 to 1 micron together with small amounts of a siliceous filler with a particle size distribution between about 0.01 and 0.1 microns. This latter is added to adjust the handling properties of the paste. The total amount of filler contained in such a composition to give a consistency which is clinically useful is commonly around 75%, but may be as high as about 80% in some cases. Typical physical properties are a yield strength around 130 MPa, a Vickers hardness around 70, and shrinkage on cure of about 2.5 to 3.0%. The Shore A hardness of the uncured paste is used as a measure of "packability" and "handling characteristics" of the paste, and it has been determined empirically that for filling materials which are to be used in posterior cavities an optimum value for the Shore A hardness is between about 50 and 55. A paste made as above typically has a Shore A hardness of around 30 to 45. In the present invention, a paste as above is taken and mixed with an additional fraction of filler chosen such that the mean particle size of this additional filler is at least about twenty times the size of the largest filler in the paste, and is preferably mono-modal. In practice the particle size of this additional filler will have a distribution, but the largest and smallest particles in this filler should preferably be within about 25% of the mean size. Thus in the above example, the largest particle size contained in the paste is 1 micron, and the mean size of the additional filler should therefore be at least about 20 microns, with no particles larger than 25 microns or smaller than 15 microns. However, the additional filler may also be larger, for example with a mean size of about 65 microns. In this case the largest and smallest particles contained in the filler should be around 85 microns and 50 microns respectively. Such a filler

fraction may conveniently be made by passing milled glass through commercially available sieves.

The following examples serve to illustrate the invention further, but are not restrictive in any way. Since the materials described in the examples are sensitive to and hardened by exposure to light between 400 and 500 nm, all preparations were done in yellow light devoid of light in this wavelength range. In the following examples "parts" means "parts by weight".

Example 1

Preparation of the initial paste

A resin mixture was first made by combining urethane resin 44 parts, TCB resin 34 parts, trimethylolpropane trimethacrylate 20 parts, camphor quinone 0.28 parts, dimethylaminobenzoic acid ethyl ester 0.59 parts, butylated hydroxytoluene 0.1 parts, hydroquinone monomethylether 0.025 parts, and 2-hydroxy-4-methoxybenzophenone 1.0 part in a flask and stirring at 50°C until a clear homogenous mixture was obtained.

This resin (25.3 parts) was then mixed at 50°C with 74.7 parts of a powder mixture comprising silanated strontium glass with a mean particle size of 0.8 microns 94.5 parts, strontium fluoride 5 parts, and hydrophobic fumed silica (particle size range about 0.05 microns) 0.5 parts, to give a stiff paste after cooling. The overall filler content of this paste is 74.7% by weight. The properties of this paste were measured and results are given in Table 1

Example 2

Preparation of a the addition filler with narrow particle size distributions

Glass frit with a particle size of about 2 to 5 mm was milled in a dry ball mill to give a powder with a particle size ranging from about 1 micron to 1

mm and a mean particle size of about 50 microns. This was sieved over a mesh with an aperture size of 250 microns, and the coarse fraction remaining in the sieve was discarded. The glass which passed through was sieved over a mesh with an aperture of 100 microns to obtain a fraction with a particle range between 100 and 250 microns. This is termed fraction A. The remaining glass was sieved over a mesh with an aperture of 85 microns, and the glass remaining in the sieve was discarded. The glass which passed through was collected and sieved over a mesh with an aperture size of 48 microns, the fraction which passed through being discarded. In this way a fraction with a particle size range of 48 to 85 microns was obtained. This is termed fraction B. Both fractions A and B were separately silanated by slurring them at room temperature with 3-(trimethoxysilyl)propyl methacrylate (1% of the weight of the glass) dissolved in water acidified with acetic acid. After one hour the glass fractions were filtered off and dried for 18 hours at 85°C in an oven.

Example 3

Preparation of a first paste containing additional filler fraction B

UK221581

Two hundred grams of the paste from example 1 was taken and mixed at 50°C with 160 grams of silanated glass fraction B from example 2 using a planetary mixer. After mixing for 15 minutes the paste had formed a coherent mass. This was cut up and was spread around the mixing pot before being mixed for a further 15 minutes. The paste mass was again cut up, spread around the pot and mixed for 15 minutes, but this time a vacuum of 220 mbar was applied for the last 10 minutes. The resulting paste when cool was only marginally stiffer than the original paste from example 1 even

though it contained a total of 86% filler by weight. The properties of the paste were measured and these are given in Table 1.

Example 4**Preparation of a second paste containing additional filler fraction B**

UK221591

The paste from example 3 (342 grams) was taken and 13 grams of silanated glass from example 2 fraction B was added using the procedure as given in example 3. This paste contained a total of 86.5% filler. The properties were measured and results are given in Table 1.

Example 5**Preparation of a third paste containing additional filler fraction B**

UK221592

Paste from example 4 (293 grams) was taken and 12 grams of silanated glass from example 2 fraction B was added using the procedure as given in example 3. This paste contained a total of 87.0% filler. The properties were measured and results are given in Table 1.

Example 6**Preparation of a fourth paste containing additional filler fraction B**

UK221592

Paste from example 5 (265 grams) was taken and 10 grams of silanated glass from example 2 fraction B was mixed in using the procedure as given in example 3. This paste contained a total of 87.5% filler. The properties were measured and results are given in Table 1:

WO 00/61073

PCT/US00/08709

Example 7**Preparation of a fifth paste containing additional filler fraction B**

UK221593

Paste from example 6 (235 grams) was taken and 10 grams of silanated glass from example 2 fraction B was mixed in using the procedure as given in example 3. This paste contained a total of 88.0% filler. The properties were measured and results are given in Table 1.

Example 8**Preparation of a first paste containing additional filler fraction A**

UK221511

One hundred grams of the paste from example 1 was taken and mixed at 50°C with 158.3 grams of silanated glass fraction A from example 2 using a planetary mixer. After mixing for 15 minutes the paste had formed a coherent mass. This was cut up and was spread around the mixing pot before being mixed for a further 15 minutes. The paste mass was again cut up, spread around the pot and mixed for 15 minutes, but this time a vacuum of 220 mbar was applied for the last 10 minutes. The paste contained a total of 90% filler, but was judged to be too dry and stiff. A further 10 grams of the paste from example 1 was therefore added and the mixing procedure outlined above repeated. The resulting paste contained a total of 89.6% filler by weight. The properties of the paste were measured and these are given in

Table 1.

Example 9**Preparation of a second paste containing additional filler fraction A**

UK221541

The paste from example 6 (233.7 grams) was taken and warmed to 50°C in a planetary mixer. Silanated fraction A from example 2 (10.31 grams) was added and the mixing procedure carried out as outlined in example 3. This paste contained a total of 89% filler. The properties of the paste were measured and these are given in Table 1.

Example 10**Preparation of a third paste containing additional filler fraction A**

UK221542

The paste from example 7 (199 grams) was taken and warmed to 50°C in a planetary mixer. Silanated fraction A from example 2 (14.96 grams) was added and the mixing procedure carried out as outlined in example 3. This paste contained a total of 88.6% filler. The properties of the paste were measured and these are given in Table 1.

Example 11**Preparation of a paste containing an additional filler fraction with spherical particles**

UK221671

Spherical glass beads with a particle size ranging from 40 to 70 microns were silanated by slurring them at room temperature with a solution of 3-(trimethoxysilyl)propyl methacrylate (1% of the weight of the glass) in water acidified with acetic acid. After one hour the glass spheres were filtered off and dried for 36 hours at 85°C in an oven. Two hundred grams of the

paste from example 1 were mixed with two hundred and twenty two grams of these silanated spheres following the procedure in example 3. The resulting paste felt only marginally stiffer than the paste from example 3 even though it contained an extremely high total solid filler content of 88%. The properties were measured and the results are given in Table 1. It is notable that the Shore A hardness value of this paste was only 3 units higher than that of the starting paste, even though the solid filler content of the two pastes differed by 13%.

Example 12**Preparation of a second paste containing an additional filler fraction with spherical particles**

UK221681

The paste from example 11 (382 grams) was mixed as described in example 3 with further silanated glass spheres (34.4 grams). The result was a stiff paste which was nevertheless easily spatulated and clinically adaptable to a tooth surface. The properties were measured and the results are given in Table 1.

Example 13**Preparation of a second paste containing an additional filler fraction with both spherical and Irregular shaped particles**

UK221722

The filler fraction B was mixed with an equal weight of the spherical filler as used in example. A paste was produced containing 88.5% total weight percent filler, using the method as in example 3. The properties are given in Table 1.

Comparative example 1 using additional filler with a wide particle size distribution

UK221631

The glass powder used in example 2 was taken, passed through a 250 micron sieve to remove coarse particles, and silanated as described in example 2. This silanated glass powder (100 grams) was added to the paste from example 1 (200 grams) using the mixing procedure described previously in example 3. The resulting paste contained a total of 83.1% filler and was a very stiff paste. A further 10 grams of the silanated glass powder above was added and the mixing procedure repeated. The resulting paste contained a total of 83.7% filler and was dry, crumbly and only just coherent. It was not possible to add more glass and still obtain a cohesive paste. The properties were measured and results are given in Table 1. This paste is cannot be extruded from a dental syringe.

Measurement of extrusion force

Dental syringes (Hawe-Neos Dental, CH-6934 Bioggio, Switzerland, article number 436) with an internal tip diameter of 2 mm were filled with the material to be tested. After allowing the syringe and contents to equilibrate to 23°C, the syringes were mounted in a universal testing machine (Zwick) and the material extruded by pushing the piston into the syringe at a constant velocity of 28 mm per minute. The force on the piston, or extrusion force, was noted. At least three measurements for each material were taken and the average extrusion force was calculated. Further syringes were tested by hand, and the ability to extrude the paste from the syringe judged from the hand force needed.

Measurement of yield strength

Metal forms with an internal diameter of 4 mm and a height of 6 mm as described in ISO 9917 section 7.4 were used to prepare the specimens. The paste to be measured was filled into the forms, covered with polyester foil, and pressed with metal plates to extrude excess material. The material was then cured for 40 seconds from each end using a dental curing lamp (Spectrum Lite, Dentsply) with an output between 600 and 700 mW/cm². The forms complete with specimen were drawn across silicon carbide paper (600 grit) until a smooth surface level with the end of the form was obtained, and then the cured specimens were removed from the form. The specimens were stored in water at 37°C for 24 hours before being tested in a universal testing machine (Zwick) with a crosshead speed of 1 mm/minute. The stress strain curve for each specimen was inspected and found to consist essentially of an initial straight portion followed by a curved portion leading to the final breaking point. The straight portion of the curve corresponds to elastic behaviour of the material, whereas the curved portion corresponds to plastic flow. The force at which the stress strain curve first deviated from a straight line was taken as the yield point. The yield point is expressed in MPa, and is calculated by dividing the yield force in Newtons by the cross-sectional area of the specimen. The average value of at least five specimens for each material was calculated.

Properties of the pastes		% filler	Yield str. MPa	Vickers hardness HV5	Shrinkage volume %	Shore A hardness of paste	Extrusion force Newtons	Extrusion by hand
Material from example								
1	74.7	154.4	63.7	2.6	46.8	92.0		Easily extrudable
3 (UK221581)	86.0	200.0	78.9	1.8	53.2			Extrudable
4 (UK221591)	86.5	200.0	87.2		54.6			Extrudable
5 (UK221592)	87.0	203.9	95.6	1.5	57.6	290		Extrudable
6 (UK221593)	87.5	205.2	95.7		62.2			Extrudable but stiff
7 (UK221611)	88.0	215.6	94.5	1.4	64.8			Extrudable but stiff
8 (UK221511)	89.6	198.0	77.0	1.1	75.0			Not extrudable
9 (UK221541)	89.0	197.0	68.6		68.2			Not extrudable
10 (UK221542)	88.6	195.0	67.9	1.3	68.8			Just extrudable
11 (UK221671)	88.0	188.4	71.5		49.0	120.0		Easily extrudable
12 (UK221681)	89.0	191.1	62.4			56.0		Easily extrudable
13 (UK221722)	89.5	192.3			1.2	51.8		Easily extrudable
Comparative example 1 (UK221631)	93.7	205.0	68.3	1.8	63.6	>500		Not extrudable

Table 1

From Table 1 it can be seen that the conventional paste of example 1 has a yield strength of only 154 MPa, a Vickers hardness of 63.7, a volume shrinkage of 2.6%, and an extrusion force from a dental syringe of 92 Newtons. This paste may therefore be easily extruded from a dental syringe, but has an unacceptably high shrinkage as well as low surface hardness and low yield strength.

When the filler loading is increased by adding additional filler with a conventional particle size distribution as in comparative example 1, the yield strength is improved and the shrinkage is reduced below 2%, but the surface hardness is barely changed and the paste becomes so stiff that it can no longer be extruded from a dental syringe.

In contrast the formulations from examples 3, 4, 5, 6, and 7, which fall within the scope of the present invention have improved yield strengths, improved surface hardness, reduced volume shrinkage, and are also extrudable from a dental syringe.

The present invention therefore allows the formulation of pastes with required optimum properties of yield strength, surface hardness and extrudability from a dental syringe, which are not otherwise possible. Particularly desirable are formulations comprising additional fillers comprising both spherical and irregular shaped particles. Different methods of particle size measurement give different results, and the values given for purposes of the present invention are determined by sieving.

Claims:**What is claimed is:**

1. An intra-oral or extra-oral dental restorative material comprising:
 - a) at least one polymerizable monomer
 - b) a first solid filler component with a mean particle size between about 0.1 and about 5 microns
 - c) a second solid filler component with a mean particle size at least twenty times greater than the largest particle in the first solid filler component, and a particle size distribution such that at least about 80 percent of the particles in this second filler component are within the range of 75 to 125 percent of its mean size, determined by sieving.
2. A material as in claim 1 in which 90 percent of the particles in the second filler component are within the range of about 75 to about 125 percent of its mean size, determined by sieving.
3. A material as in claim 1 in which all of the particles in the second filler component are within the range of about 75 to about 125 percent of its mean size, determined by sieving.
4. A material as in claim 1 comprising from about 5 to about 25 percent by weight of said polymerisable monomer.
5. A material as in claim 1 comprising from about 10 to about 15 percent by weight of said polymerisable monomer.

6. A material as in claim 1 wherein the Vickers hardness of the cured material is greater than about 90, and the yield strength is at least about 180 MPa.
7. A material of claim 1 wherein at least one of the solid filler components comprises a fluoride containing glass.
8. A material of claim 1 wherein at least a portion of one of the solid filler components comprises spherical or essentially spherical particles.
9. A material of claim 1 wherein the first or second solid filler comprises fluoride containing glass.
10. A material of claim 1 wherein at least one fraction of the solid filler comprises spherical or essentially spherical particles comprising a fluoride containing glass.
11. A material of claim 1 which additionally contains between 0 and 5 percent of an solid filler having a mean particle size from about 1 to 100 nm.
12. A material of claim 1 wherein the extrusion force of the material from a dental syringe with a tip diameter of 2 mm is less than 300 Newtons.
13. A material of claim 4 wherein the extrusion force from a dental syringe with a tip diameter of 2 mm is less than 300 Newtons.

INTERNATIONAL SEARCH REPORT

International Application No
PCT/US 00/08709

A. CLASSIFICATION OF SUBJECT MATTER

IPC 7 A61K6/083

According to International Patent Classification (IPC) or to both national classification and IPC

B. FIELDS SEARCHED

Minimum documentation searched (classification system followed by classification symbols)
IPC 7 A61K

Documentation searched other than minimum documentation to the extent that such documents are included in the fields searched

Electronic data base consulted during the international search (name of data base and, where practical, search terms used)

EPO-Internal, PAJ

C. DOCUMENTS CONSIDERED TO BE RELEVANT

Category	Citation of document, with indication, where appropriate, of the relevant passages	Relevant to claim No.
A	EP 0 530 926 A (KANEBO LTD ;MITSUBISHI CHEM IND (JP)) 10 March 1993 (1993-03-10) page 4, line 51 -page 5, line 55	1-13
A	EP 0 060 911 A (BLENDAX WERKE SCHNEIDER CO) 29 September 1982 (1982-09-29) page 3, paragraph 2 - paragraph 3 example 1	1-13
A	GB 1 544 776 A (MINNESOTA MINING & MFG) 25 April 1979 (1979-04-25) page 2, left-hand column, line 47 -right-hand column, line 2 page 3, left-hand column, line 12 - line 35	1-13
	-/-	

Further documents are listed in the continuation of box C.

Patent family members are listed in annex.

* Special categories of cited documents :

- "A" document defining the general state of the art which is not considered to be of particular relevance
- "E" earlier document but published on or after the international filing date
- "L" document which may throw doubts on priority claim(s) or which is cited to establish the publication date of another citation or other special reason (as specified)
- "O" document referring to an oral disclosure, use, exhibition or other means
- "P" document published prior to the international filing date but later than the priority date claimed

- "T" later document published after the international filing date or priority date and not in conflict with the application but cited to understand the principle or theory underlying the invention
- "X" document of particular relevance; the claimed invention cannot be considered novel or cannot be considered to involve an inventive step when the document is taken alone
- "Y" document of particular relevance; the claimed invention cannot be considered to involve an inventive step when the document is combined with one or more other such documents, such combination being obvious to a person skilled in the art.
- "Z" document member of the same patent family

Date of the actual completion of the international search

11 July 2000

Date of mailing of the international search report

21/07/2000

Name and mailing address of the ISA

European Patent Office, P.B. 5818 Patentlaan 2
NL - 2280 HV Rijswijk
Tel. (+31-70) 340-2040, Tx. 31 651 epo nl.
Fax: (+31-70) 340-3016

Authorized officer

Cousins-Van Steen, G

INTERNATIONAL SEARCH REPORT

National Application No
PCT/US 00/08709

C.(Continuation) DOCUMENTS CONSIDERED TO BE RELEVANT

Category *	Citation of document, with indication, where appropriate, of the relevant passages	Relevant to claim No.
A	US 4 649 165 A (KUHLMANN WERNER) 10 March 1987 (1987-03-10) cited in the application column 3, line 39 - line 55 column 4, line 9 - line 31 <hr/>	1-13
A	EP 0 053 442 A (ICI PLC) 9 June 1982 (1982-06-09) page 2, line 10 -page 3, line 28 page 13, line 30 - line 31 <hr/>	1-13

INTERNATIONAL SEARCH REPORT

Information on patent family members

National Application No

PCT/US 00/08709

Patent document cited in search report	Publication date	Patent family member(s)		Publication date
EP 0530926 A	10-03-1993	JP 2732968 B JP 5058837 A CA 2077734 A DE 69210144 D DE 69210144 T US 5350782 A		30-03-1998 09-03-1993 07-03-1993 30-05-1996 28-11-1996 27-09-1994
EP 0060911 A	29-09-1982	AT 13808 T DE 3170993 D JP 57169410 A US 4427799 A		15-07-1985 25-07-1985 19-10-1982 24-01-1984
GB 1544776 A	25-04-1979	AU 508664 B AU 2204977 A CA 1103388 A CH 630524 A DE 2705220 A FR 2340085 A JP 52098391 A JP 63047682 B SE 458906 B SE 7700202 A		27-03-1980 17-08-1978 16-06-1981 30-06-1982 11-08-1977 02-09-1977 18-08-1977 26-09-1988 22-05-1989 10-08-1977
US 4649165 A	10-03-1987	DE 3403040 A AT 40945 T DE 3568396 D WO 8503220 A EP 0156105 A JP 5045564 B JP 61501090 T		08-08-1985 15-03-1989 06-04-1989 01-08-1985 02-10-1985 09-07-1993 29-05-1986
EP 0053442 A	09-06-1982	AR 229517 A AT 15593 T AU 555712 B AU 7760981 A CA 1189996 A DE 3172366 D DK 525081 A, B, ES 507683 D ES 8304428 A FI 813861 A, B, GR 75760 A HU 193515 B IE 51828 B IL 64386 A JP 1970245 C JP 4048764 B JP 57120506 A NO 813926 A, B, NZ 199140 A PT 74069 A, B US 4407984 A ZA 8107967 A		15-09-1983 15-10-1985 09-10-1986 10-06-1982 02-07-1985 24-10-1985 04-06-1982 01-03-1983 01-06-1983 04-06-1982 02-08-1984 28-10-1987 01-04-1987 29-11-1985 18-09-1995 07-08-1992 27-07-1982 04-06-1982 20-03-1985 01-01-1982 04-10-1983 29-09-1982